

Technical articles

Oxygen sensor signal validation for the safety of the rebreather diver

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Key words

Rebreathers/closed circuit, oxygen, monitoring device, equipment

Abstract

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In electronically controlled, closed-circuit rebreather diving systems, the partial pressure of oxygen inside the breathing loop is controlled with three oxygen sensors, a microcontroller and a solenoid valve – critical components that may fail. State-of-the-art detection of sensor failure, based on a voting algorithm, may fail under circumstances where two or more sensors show the same but incorrect values. The present paper details a novel rebreather controller that offers true sensor-signal validation, thus allowing efficient and reliable detection of sensor failure. The core components of this validation system are two additional solenoids, which allow an injection of oxygen or diluent gas directly across the sensor membrane.

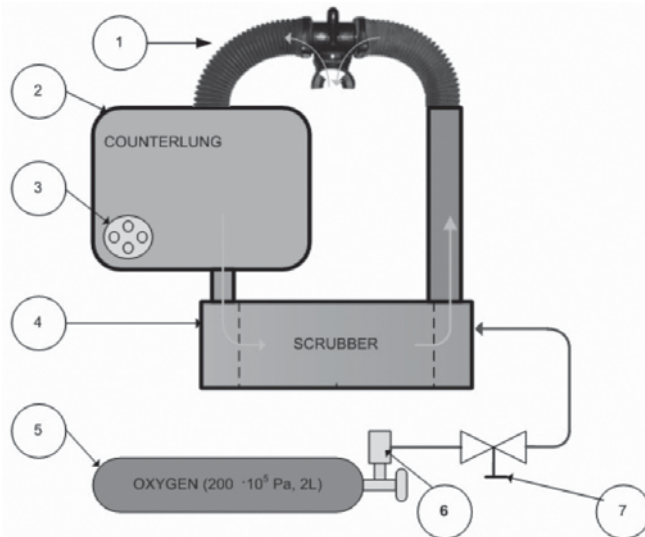
Introduction

REBREATHING SYSTEMS

Closed-circuit rebreather (CCR) diving with its many advantages in comparison to open-circuit diving is becoming increasingly popular.¹ In an oxygen (O₂) rebreather (Figure 1) the diver exhales into a bag – the so called 'counterlung'.² A scrubber removes carbon dioxide (CO₂) and fresh gas is added to replace metabolized oxygen (O₂). This recycled gas is then inhaled by the diver again. In the case of a pure O₂ rebreather, the circuit contains mainly O₂. Thus the partial pressure of O₂ (ppO₂) inside the circuit is dependent on the ambient pressure (Dalton's Law). Such a rebreather has the advantages of maximizing the efficiency of gas usage, and provides bubble-free, silent diving and warm, humid breathing gas. The presently recommended ppO₂ limits for life-sustaining breathing gas range from 0.1 bar (10.1 kPa) to 1.6 bar (162 kPa).^{*} A ppO₂ above this upper limit may lead to acute oxygen toxicity, manifested as an epileptiform convulsion, which is likely to be fatal underwater. A ppO₂ below 0.1 bar (10.1 kPa) will lead to unconsciousness.^{3,4} The maximum ppO₂ limit recommended varies from 1.4–1.6 bar, and sets the depth limit for pure O₂ and mixed-gas rebreathers. Rebreathers are classified into either semi-closed-circuit rebreathers (SCR) or manually or electronically controlled closed-circuit rebreathers (mCCR or eCCR).^{5,6} In an SCR, O₂-enriched gas enters the breathing loop via a constant flow injector (commonly an orifice, typically 6–12 bar L.min⁻¹) to substitute the metabolized O₂ (Figure 1). Excess gas in the circuit is then vented through an overpressure valve. The maximum depth for an SCR is mainly limited by the percentage of O₂ in the supply gas.

In a CCR, the ppO₂ is usually kept at a constant level, only the metabolized O₂ is substituted. In mixed-gas diving, the breathing gas in a CCR contains nitrogen (N₂) or helium (He) or, for deeper dives, a He-N₂ mixture. To maintain the ppO₂ at a constant level, a control loop is needed.^{7,8} Therefore, electrochemical oxygen sensors, whose output signals are proportional to the ppO₂, are used as sensing elements. In a mCCR, the diver reads the ppO₂ from a display, then, as necessary, adjusts the O₂ injection needle valve and/or adds O₂ manually. In an eCCR this control task is usually performed by a microcontroller and a solenoid valve.

Figure 1
Schematics of an oxygen rebreather
1: mouthpiece, 2: counterlung, 3: overpressure valve,
4: CO₂ scrubber, 5: oxygen cylinder, 6: pressure
regulator, 7: manual valve



Footnote: * In this report, pressure is expressed as bar pressure (1 bar = 0.1013 MPa, 101.3 kPa)

Both types of closed rebreather systems have many advantages:

- Gas efficiency: Open-circuit scuba diving has a low gas utilisation efficiency from less than 5 % on the surface, to below 0.5 % at 100 metres' sea water (msw) depth. In CCRs, because the breathing gas is recycled and, under optimal conditions, only the metabolised O₂ is replaced, gas efficiency may approach 100 %, enabling the design of comparatively small, lightweight systems where gas costs and supply are no longer the limiting factors.
- Silence: CCRs allow bubble-free, silent diving; only during ascent gas is vented from the circuit.
- Warm, humidified breathing gas: Gas from open-circuit scuba is dry and, because of expansion of the gas in the regulator, cold. Cold breathing gas cools the diver and, in very cold water, may lead to regulator malfunction due to freezing. In a rebreather, the breathing gas is usually warm and humid, as the chemical CO₂ absorption produces water and heat as by-products. However, in cold water, scrubber efficiency can also be impaired.

REBREATHER SAFETY

To ensure the safety of the diver, rebreathers sold within the European Union have to be CE-marked (European Normative EN14143:2003),⁹ and are classified as Category III Personal Protective Equipment. They must be certified by an independent, certified Notified Body.¹⁰

Unfortunately there is already a long list of rebreather diving incidents and fatalities.^{1,11,12} The most commonly identified systems failures in these deaths are:

- ppO₂ outside of life-sustaining limits
- high CO₂ levels
- water leakage into the breathing circuit.

High CO₂ levels can be avoided by good scrubber design and conservative scrubber management. The latest developments use pre-packed scrubbers, to avoid poor scrubber filling methods that may cause channeling, an important cause of raised CO₂ levels in the breathing circuit. Water leaking into the circuit reacts with the scrubber chemicals, causing the so called 'caustic cocktail'. Some CCRs avoid this by incorporating hydrophobic membranes in the inlet and outlet of the scrubber, that prevent water from entering or leaving.

Figure 2 details the ppO₂ control in an eCCR. A solenoid stuck in either the open or closed positions is a typical failure of the O₂ injection system. A properly trained diver will be able to handle this and other emergency situations. The state of the art for the electronic components is to use redundant design; typically the diver carries two or three independent ppO₂ meters and several displays, the ppO₂ inside the loop depending on the accuracy and reliability of the sensor signals.

O₂ SENSORS

In current rebreathers, galvanic O₂ sensors are used. The core element of a galvanic O₂ sensor is an electrochemical cell ('fuel cell') consisting of two electrodes of dissimilar metals (cathode – a noble metal behind a diffusion barrier, usually of Teflon; anode – lead) in contact with a liquid or semisolid basic electrolyte, usually potassium hydroxide. When the sensor is exposed to the breathing gas, O₂ diffuses through the Teflon membrane and is chemically reduced at the surface of the cathode to hydroxyl ions. The hydroxyl ions then flow toward the lead anode, where an oxidation reaction occurs generating an electrical current proportional to the ppO₂.

In most cases, a resistor is incorporated in the electrical circuit, thus the output from the sensor is measured in mV. Many sensors incorporate temperature compensation in the electronics. Typical specifications for an O₂ sensor for diving purposes are:

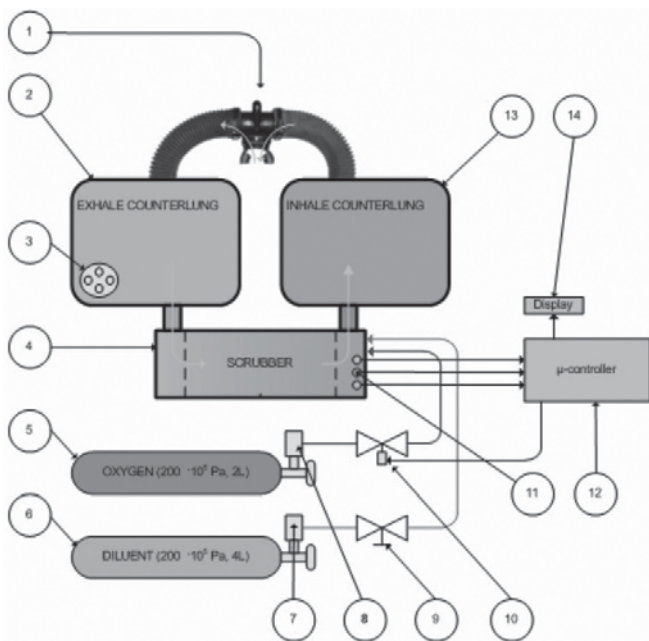
- Range: 0–100% O₂, 0–2 bar O₂
- Signal output: 8–13mV @ 0.21 bar O₂ (linear slope: 40–75 mV per bar pressure)
- Response 90%: 6 s

In the reaction with O₂, the anode is consumed, which is the limiting factor determining the lifetime of the sensor, typically 12–24 months.

O₂ SENSOR FAILURES

Typical O₂ sensor failures are:

Figure 2
Schematics of an electronic closed-circuit rebreather
1: mouthpiece, 2: exhale counterlung,
3: overpressure valve, 4: CO₂ scrubber,
5: oxygen cylinder, 6: diluent cylinder,
7, 8: pressure regulators, 9: manual diluent valve,
10: solenoid, 11: ppO₂ sensors, 12: microprocessor,
13: inhale counterlung, 14: display



- non linearity
- current limitation (the output signal of the sensor is limited, thus will remain constant at a certain ppO_2)
- slow signal response
- other sensor failures (mechanical or electrical damage).

The most common failure mode is not achieving the correct electrical output for a given ppO_2 . This is due either to exhaustion of the anode or loss of water from the electrolyte solution, resulting in a low reading. The most serious failure is not giving the correct output above a given ppO_2 . Exhaustion of the anode surface results in an increase in the response time and then what is called current limitation, voltage limitation, or ceiling fault. Sensors can fail temporarily if the sensor membrane is exposed directly to water. This results in a dramatic increase in the response time and sensor readings that are too low. This problem can be avoided by good design, such as where the sensors are mounted top down, so that water cannot collect on the sensor membrane. Damage of the sensor membrane due to impact shocks may lead to electrolyte leakage, which usually results in an increased current output.

Failure of the electronic components may lead to several problems. Oxygen sensors generate an electrical charge, which is drained via a resistive load; in the case of a failed resistor this charge will build up until current leakage is sufficient to dissipate the charge generated: this can be as high as 100V. With a thermistor failure, the output may vary by up to 2% per degree Celsius. In the case of a shortcut of the resistor, the sensor will produce no output. Other sensor failures that may occur temporarily are current changes caused by fast decompression and He and CO_2 susceptibility.

Non-linearity and current limitation are the most serious failures for a rebreather diver; for example, a current-limited cell may report a ppO_2 of 1.2 bar correctly, but a ppO_2 above this will not be correctly indicated. This is despite calibration with 100% O_2 on the surface showing normal values. This causes injection of more O_2 , resulting in a potentially dangerous elevation of ppO_2 inside the circuit outside of life-sustaining limits. For these reasons, multiple, typically three, O_2 sensors are used together with a 'voting algorithm'.^{13,14} Here, the sensor signals are continuously compared with each other. If one sensor signal differs from the others, that sensor signal is 'voted out'. In such a case, the two remaining sensors are used for further control of the system and the user is notified with an alarm signal. For example, in the Hammerhead™ CCR electronic (Juergensen Marine, USA) a sensor is voted out if its signal deviates by more than 15% from the average value of the other two sensors. As the voting algorithm is based on a comparison of sensor signals, it will fail when two or more sensors give the same but incorrect signals; this cannot be reliably detected with the voting algorithm. Unfortunately similar concurrent sensor failures do occur, especially when sensors from

the same manufacturer and same production lot are used. Rebreather divers have tended to replace all the sensors at the same time with the same type of sensor. This practice is now changing so that sensors from different production lots and/or manufacturers are used and additional checks are performed. Pre-dive preparation currently includes a single-point normobaric calibration with 100% O_2 or air. Since during diving a ppO_2 above 1.0 bar will occur, this is not optimal. Some rebreather divers now pressure test sensors at 1.6 bar to check linearity.

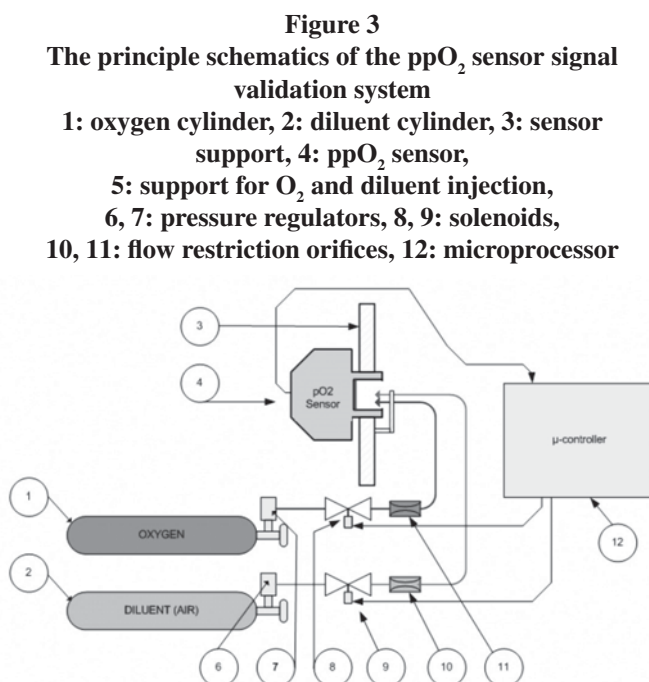
The present work details an alternative to the voting algorithm, in which a novel sensor signal validation concept allows reliable detection of sensor failure and automatic sensor calibration without any interaction by the user.

Methods

OXYGEN SENSOR SIGNAL VALIDATION

The principle of the sensor signal validation technique is based on injection of a gas with a known O_2 fraction across the O_2 sensor membrane. As the actual depth is known from the readings of the pressure sensor, the ppO_2 of the injected gas can be calculated. The injected gas flushes the sensor membrane, so that the ppO_2 of the injected gas is read, not that of the breathing gas in the circuit. The sensor readings can then be compared to the theoretically calculated values, confirming whether or not the sensor is working correctly. Any O_2 sensor suitable for diving applications may be used with this sensor validation method.

Figure 3 shows the practical setup of the sensor signal validation apparatus to allow flushing the sensor membrane with O_2 or with diluent. Two solenoids are incorporated for



the flow control. In some previous CCR units, a similar device to flush the sensor membrane manually with diluent could be found, but frequent cell failures have been reported with this technique. This is likely to be a result of the injection of gas at intermediate pressure (8–10 bar above ambient) directly onto the sensor membrane, possibly shooting moisture drops on the orifice at the sensor at high velocity. To avoid this problem in the new system, orifices with an internal diameter of 140 μm are mounted on the exit of the solenoids reducing the gas velocity at the output and limiting the gas flow to approximately 2 bar $\text{L}\cdot\text{min}^{-1}$.

Sensor signal validation with diluent is carried out every 120 s (default setting, range 60–255 s). In addition to that, in a depth range of 0–10 msw the same procedure can be carried out with O_2 . This allows detection of non-linearity and/or current limitation of the sensor when combined with periodic checks with diluent allowing calibration of the sensor at a ppO_2 greater than 1 bar. By analysis of the signal response the t_{90} response time can be calculated, which also allows recognition of slow response times. The typical duration of flushing the sensor membrane is 6 s, which results in 0.2 bar L of injected gas. Considering a total circuit volume of about 6 L, the signal validation procedure with air causes a decrease of ppO_2 inside the circuit of approximately 0.01 bar; with 100 % O_2 , it will lead to an increase of the ppO_2 of 0.016 bar.

The ppO_2 control in the first prototype was designed to keep the oxygen fraction (FO_2) in the circuit constant at 0.50 to a maximum depth of 14 msw. Below that depth, the ppO_2 has a set point of 1.2 bar. If a failure is detected, the diver is notified via an alarm. The diver should then change to an independent bailout system and abort the dive. Theoretically safe operation can be achieved with just one sensor with this sensor signal validation system. However, for redundancy purposes, the first prototypes included two O_2 sensors along with the electronics and the solenoids housed inside the scrubber (Figure 4). In the case of one sensor failure, the dive can be continued. In the case of a failure of both sensors, the diver has to switch to bailout.

ELECTRONICS

Hardware

The core component of the electronics is an 8-bit RISC microcontroller (ATmega 32™, 32kByte flash ROM, 2 Kbyte RAM, Atmel™). A 4x20 characters display (EA DIP 204-4™, Electronic Assembly™, Germany) is connected via a serial peripheral interface (SPI) bus. To enable a detailed post-dive analysis a slot for SD memory cards was incorporated. Three N-FET transistors (NDS355) serve as solenoid drivers.

The microprocessors' internal 10-bit AD-converters are used for sensor signal readout. The programmable gain of 10 and 2000 is sufficient to allow a direct connection

of the two sensors (electrochemical pO_2 sensors used in rebreathers typically have a linear output with a slope of approximately 8–13 mV @ 0.21 bar ppO_2). To measure the ambient pressure/depth, two digital pressure sensors (MS5541™, Intersema™, Switzerland) are incorporated. The MS5541 is factory-calibrated for a pressure range of 0–14 bar and has a 15-bit resolution. The maximum working pressure is 33 bar (not specified), and continuous temperature compensation is built in. The sensor is read out via the SPI bus. A rechargeable battery pack (6V, 900mAh, NiMH) is used as power supply for the solenoids. For the electronic components, two low-drop voltage regulators (Texas Instruments) are used for the generation of 3.3 V and 5 V levels.

A second display is used for redundancy purposes.¹⁵ This display has analog inputs and can be connected to the O_2 sensors in parallel with the primary electronics. The core component is again an 8-bit RISC microprocessor (ATmega644p™, 64 Kbyte flash ROM, 4 Kbyte RAM, Atmel). A digital interface line is included, which allows receiving data from the primary electronics (the controller) via a serial interface (either USART or I2C). A graphics display with 128x64 characters is placed behind a concave lens ($f = 60$ mm, designed for a virtual image distance of 1 m), which allows the display to be mounted directly on the mouthpiece of the rebreather. The two displays show the sensor signal ppO_2 values, depth, central nervous system (CNS) oxygen toxicity percentage, oxygen tolerance units (OTU), diving time and decompression information.

Software

As programming platform, the Atmel AVR Studio 4™, together with the GNU C compiler WinAVR <http://winavr.sourceforge.net>, was used under Windows XP®. All sensor data are stored on the SD card in spreadsheet format. FAT 16

Figure 4
The two O_2 sensors combined with the electronics and solenoids mounted inside the scrubber in the prototype eCCR; the tubing through which diluent or 100% oxygen can be flushed to perform calibration can be seen

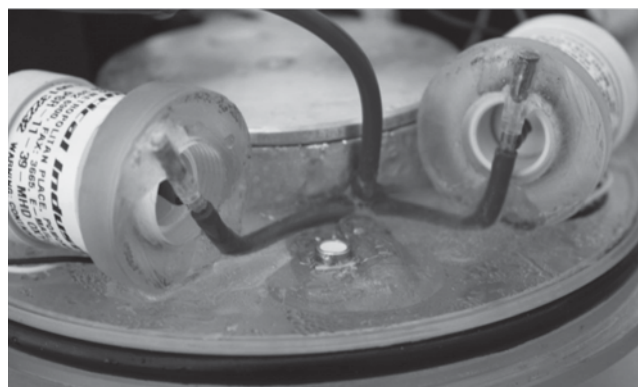
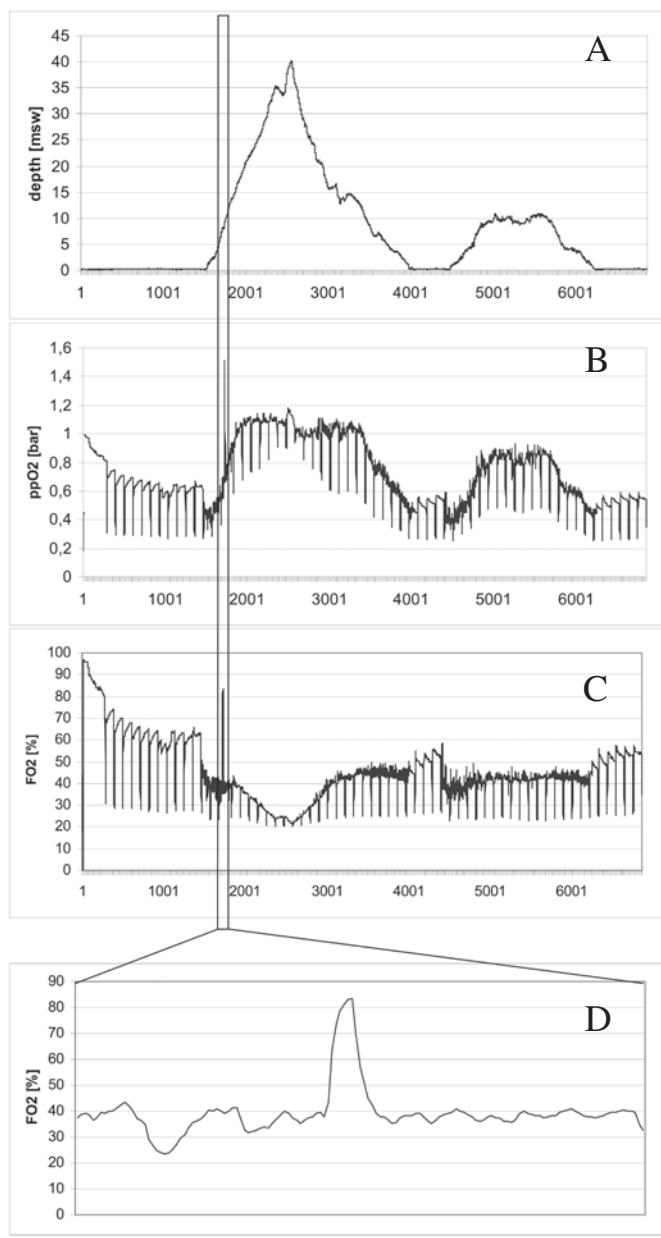


Figure 5
Data from a 100-min open-water test dive to a maximum depth of 40 msw; A: depth profile; B: ppO₂ sensor signals from two sensors; C: calculated FO₂; D: one validation cycle with 100% oxygen at 10 msw



or FAT 32 formatted SD memory cards can be used. For each dive a new file is created. Additional data, such as battery voltage, oxygen injection, oxygen consumption and error messages, are stored. These data can then be displayed with suitable programmes, such as MS Excel® (Figure 5).

Every 120 s, the sensor signal validation procedure, with diluent as the validation gas, is carried out, which results in the spikes in the readings of the ppO₂ sensors (Figure 5B-D shows the signal of one sensor). During the validation cycle the calculated FO₂ must drop to a value less than 0.25; if not, an alarm signal is generated. At a depth between 6 and

10 msw once during a dive, the sensors are checked with 100% O₂ (Figure 5D). Additional validations at depths less than 10 msw may be carried out. Error messages are created if a ppO₂ sensor signal is outside the limits set (see earlier), if the sensor signals differ by more than 0.01 bar from each other, if the battery voltage is below 6.0V and if the calculated O₂ consumption of the diver is less than 0.3 or more than 3 bar L.min⁻¹.

As the validation procedure is carried out with two different gases, it is possible to detect incorrect calibration, non linearity and slow sensor response. Because the response time of O₂ sensors is typically about 6 s (t_{90}), at the end of the validation cycle, the sensors will read, at 10 msw depth, a ppO₂ in the range of 1.6–1.9 bar rather than 2.0 bar. During the 6 s, the sensor signal output is measured every second. As the signal response has a single exponential character (the signal response time is mainly limited by diffusion of O₂ through the Teflon membrane), it is possible to forward calculate the final value. To pass the test at 10 msw, the sensors have to read a minimum 1.6 bar ppO₂ at the end of the O₂ injection and the forward calculated signal has to correspond to an O₂ fraction of greater than 90%. If the test is failed, an alarm is created and the dive should be aborted. If, despite the alarm, the dive is continued on closed circuit, for safety reasons the maximum ppO₂ set point is automatically changed to 1.0 bar. The forward calculation is applied only during the checks with 100% O₂, not for calibration or measurement purposes.

Several pre-checks have to be performed before diving with a CCR. To facilitate this, a six-step semi-automated test sequence has been implemented:

1. The user is asked to evacuate the loop of gas.
2. As soon as a pressure drop of -15 mbar is registered, the user is asked to close the mouthpiece.
3. To test for circuit leaks, the negative pressure must not fall to less than -10 mbar within the following 60 s, otherwise the test is failed.
4. After a successful negative pressure test, the loop is inflated with 100% O₂ until an overpressure of 15 mbar is registered. For the inflation, the solenoid valve opens cyclically every second for 200 ms; the cycles are counted. A correctly operating solenoid takes 45 +/- 1 cycles to inflate the counter lungs with a volume of 5 L; 42–48 counted cycles are needed to pass the test.
5. The O₂ sensors are calibrated; readings must be higher than 40 mV to pass the calibration test.
6. In step 4, the loop is inflated to +15 mbar; this pressure must not drop more than 5 mbar in 60 s to pass the test.

After successfully passing all six steps, the unit is ready to dive. If the unit is dived without a correctly passed test an alarm is created and, if the diver is still at a depth less than 6 msw, O₂ sensor calibration is immediately carried out by injection of O₂ for 15–20 s directly onto the sensor membrane. If the diver is already deeper than 6 msw, no calibration will be carried out but the maximum ppO₂

setpoint is automatically limited to 1 bar.

TESTING OF THE SENSOR SIGNAL VALIDATION ALGORITHM

For validation of the algorithm implemented on the microcontroller, a PC-based dive simulator was designed. A sensor signal simulator was developed which could be connected to the PC's printer port. Its core component is a six-channel digital potentiometer (Analog Devices™, AD5206™). Each potentiometer has a nominal value of 10 kΩ and 8-bit resolution. One of the potentiometers is connected in series with a 10 kΩ resistor to a stabilized 5 V direct-current supply for the generation of an output voltage of 0–2.5 V. For simulation of dives, the firmware of the microcontroller was slightly modified. Instead of processing the signal of the digital pressure sensors, depth information is gained from an analog to digital converter channel, by converting input voltages from 0–2.5 V to 0–100 msw depth equivalents. To simulate O₂ sensor signals in the range of 0–128 mV with a resolution of 0.5 mV, three of the potentiometers were each connected in series with a 390 kΩ resistor to the 5 V supply. The microcontroller's output usually driving the solenoids is connected to digital IO pins of a multifunction input/output board (National Instruments™, NI USB-6008™).

A graphical user interface which allows programming of the output voltages of the potentiometers at discrete time steps was developed under National Instruments LabView 7.1™. Simulation of depth profiles together with O₂ sensor signals is possible with different scenarios, such as defective O₂ sensors, being simulated with ease. Signal responses of the sensors to signal validation were pre-programmed to simulate correct function, slow response, current limitation and non linearity.

Two prototypes CCRs were designed and manufactured with the following specifications (Figure 6):

- outer dimension: 45 x 25 x 18 cm
- scrubber holds 1.8 kg of soda lime
- maximum recommended depth 40 msw (unit for recreational purposes)
- 1 oxygen cylinder: 1.5 L, 200 bar working pressure
- 1 diluent cylinder: 1.5 L, 200 bar working pressure
- total weight including cylinders: 12 kg
- maximum dive time: 180 min
- positive buoyancy: 40 N
- two O₂ sensors: PSR-11-39MD (Analytical Industries)

The implemented algorithm for sensor signal validation returns a binary validation result: either a 'correctly' or 'incorrectly' working sensor. If one of the criteria is failed, an alarm is activated.

- Validation with diluent: at the end of the validation cycle, the sensor has to read a ppO₂ corresponding to a FO₂ of less than 25%.

Figure 6
The prototype eCCR being prepared for a dive



- Validation with O₂: at the end of the validation cycle, the sensor has to read a ppO₂ corresponding to a FO₂ of at least 80%. The forward calculated sensor signal for the FO₂ has to be higher than 90%.

The sensor signal validation system was first tested in simulated dives in the laboratory, for which O₂ sensors were not required. These tests simulated O₂ sensor behaviour during normal operations to detect non-linearity, current limitation, slow response times and incorrect calibration. All the simulated sensor failures were correctly detected, validating the correct implementation of the algorithm.

TESTING THE eCCR PROTOTYPES

After laboratory testing, the function of the prototypes was tested in a hyperbaric chamber at a maximum pressure of 405 kPa and a dive duration of 40 min. The main aim of this test was the validation of the principal correct operation of the ppO₂ control and the sensor signal validation method. The second aim was to ensure that the flow rate was high enough to substitute all the gas in front of the sensor membrane with either O₂ or diluent to achieve a defined FO₂. A flow rate of 2 bar L.min⁻¹ turned out to be optimal in the current design. No system failures occurred.

Six test dives were also performed in a 10.5 metres' fresh water (mfw) research pool (Divesystem, Massa Marittima, Italy). Tests were carried out with three old sensors known to be current-limited. The faulty sensors calibrated correctly at surface, showed a correct response to the validation with diluent, but failed the validation at 10 mfw depth where their output signal reached just 1.4 bar (threshold was 1.6 bar). The failures were correctly detected.

Fifty-two open-water dives with the two prototype eCCRs were then carried out by three test divers (average depth 28 msw, range 11–52 msw). During all these dives, sensors with an age of less than one year were used. The ppO₂ control

worked flawlessly; no dive had to be bailed out on open circuit. During one dive, the handset cracked and the display inside was flooded and failed. The handset cable leading to the main controller is hermetically sealed, thus no water could reach the main electronics. The dive was successfully continued with the dive data still displayed on the head-up display. In one dive, the sensor connector became loose, resulting in a floating sensor reading. The validation with diluent successfully detected this failure and the dive was continued. An example 100-min dive to a maximum depth of 40 msw is shown in Figure 5; no sensor failures occurred and sensor signal validation cycles with O₂ and diluent (air) were successfully carried out. The present concept of ppO₂ sensor signal validation has now been incorporated into a new eCCR, the Poseidon Discovery™ MK6 rebreather.

Discussion

Like the state-of-the-art voting algorithm, the sensor signal validation method described allows reliable detection of single sensor failures. In addition to this, and unlike the voting algorithm, failures where more than one sensor shows incorrect readings can be reliably recognized. The thresholds for passing the validation procedures were found empirically. The detection of all simulated sensor signal failures proved the correct implementation of the algorithm.

As the method is based on flushing a sensor membrane with a gas with a known O₂ fraction, an interesting case is when the FO₂ in the loop is close to the FO₂ in the diluent. During validation with diluent, no sensor signal changes should occur. Safe operation of a CCR requires a diluent with a FO₂ lower than the FO₂ in the loop, thus such a case should not occur during normal operation. In the first prototype, this scenario was not investigated.

O₂ sensors have to be replaced every 1–1.5 years. By using just one or two sensors instead of three, the yearly maintenance costs are reduced without compromising safety. However, this is offset by the need for additional hardware (two solenoids plus electronics), resulting in higher production costs.

Current limitation does not appear suddenly; it is a result of the aging of the sensor. Depending on the thresholds in the O₂ validation procedure, such a sensor will, sooner or later, be recognized as faulty. Further investigation is needed with a larger batch of O₂ sensors in order to validate and adjust the thresholds for such detection to find a good compromise between conservativeness and cost effectiveness.

Conclusions

The present paper describes a novel system for sensor signal validation and reliable sensor failure detection based on flushing the sensor membranes with a gas with a known fraction/ppO₂. Injection of 100% O₂ directly onto the sensor on the surface is used for initial calibration. Then in water

up to 10 msw depth, 100% O₂ is used again to expose the sensors to a ppO₂ of up to 2.0 bar. Both current limitation and non-linearity are detected with this two-point calibration; these sensor failures do not occur temporarily, thus a single check early in the dive is sufficient. Recording the response signal of the sensor to O₂ injection also allows estimation of the sensor signal response time.

In principle, this concept allows safe operation of an eCCR with a single O₂ sensor, where, in the case of a failure, the diver must bail out of the dive. This is acceptable for a recreational unit intended for use for non-decompression dives. For more advanced diving, a second O₂ sensor should be used.

CCR diving requires continuous training and technical understanding of the equipment so that the diver is able to detect and safely handle malfunctions of the system. The validation system described in this paper facilitates rebreather handling, as the system itself is able to carry out pre-dive O₂ sensor calibration and sensor signal checks semi-automatically. Reliable automation of safety checks in an eCCR is an important step to enabling recreational divers to dive more safely using these breathing systems.

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